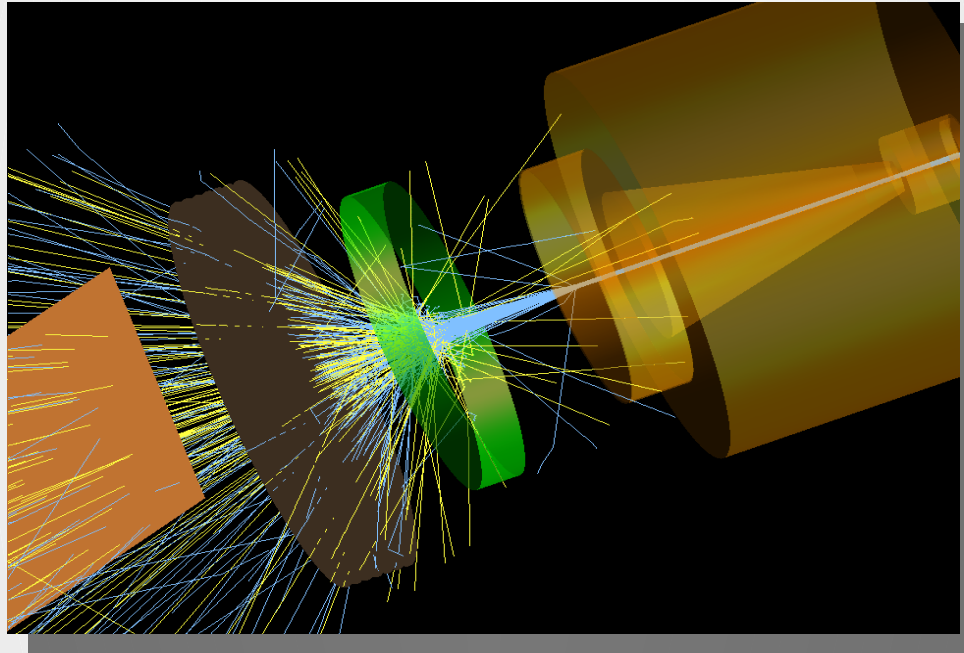


INVESTIGATION OF NESTED VOLUME-OF-INTEREST CONE-BEAM CT IMAGING WITH A LOW ATOMIC NUMBER LINEAR ACCELERATOR TARGET



Del Leary, PhD

AAPM Rocky Mountain Chapter Meeting May 20, 2016

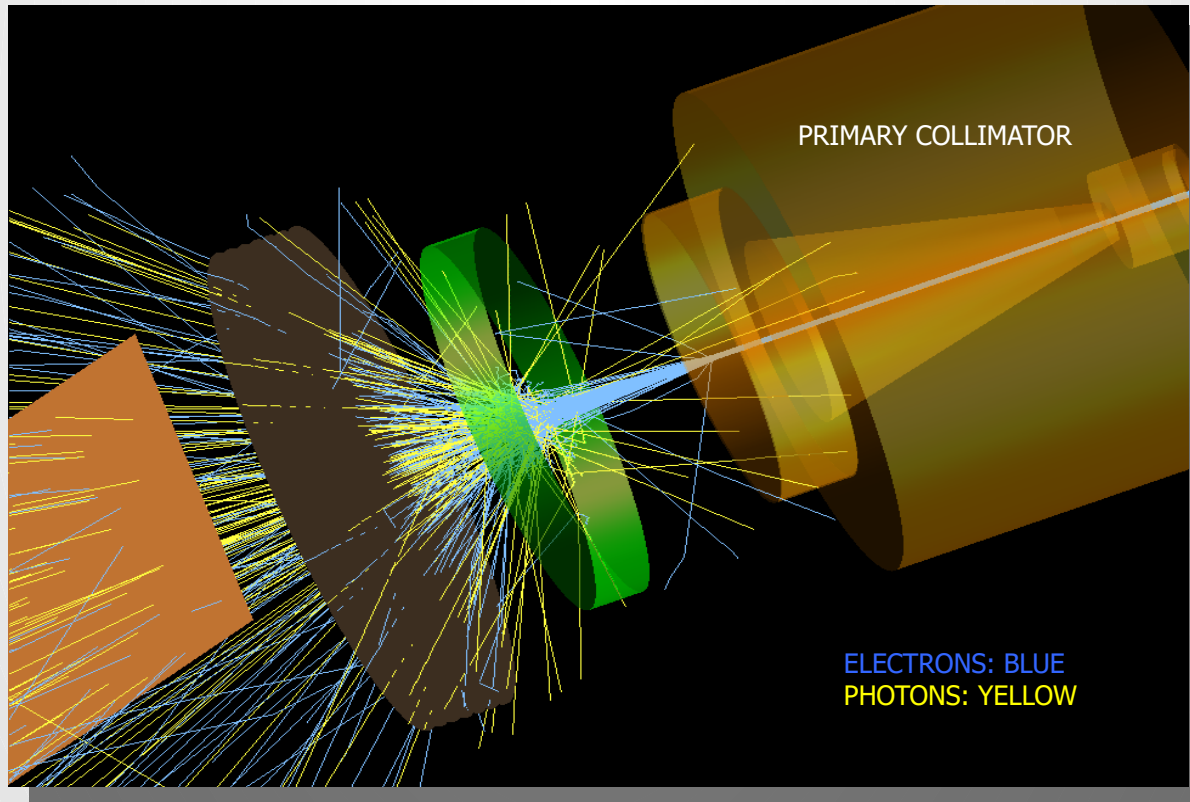


Outline

- Low Z target
- VOI
- Workflow and Utility (multiple and nested VOIs)
- Normalization and dosimetry
- Applications and future work

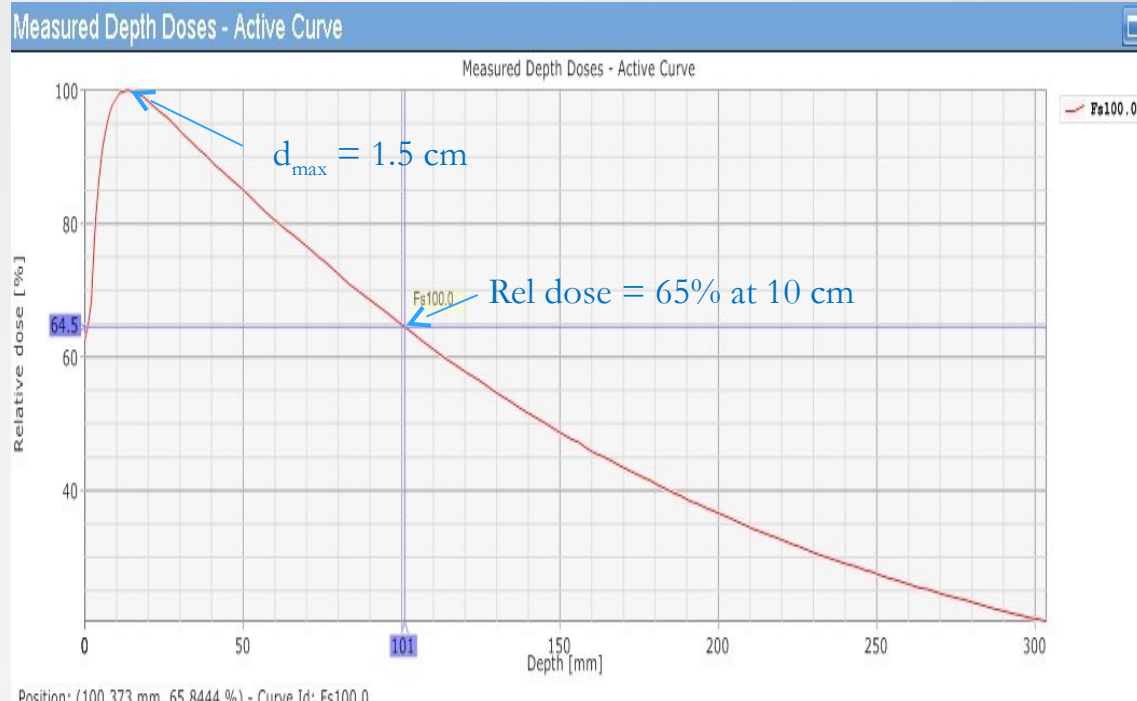
Low-Z target CBCT

- **Carbon, beryllium or aluminum target** in linac beam line
- Replaces flattening filtration
- Allows improvement of CNR by **2-5x**

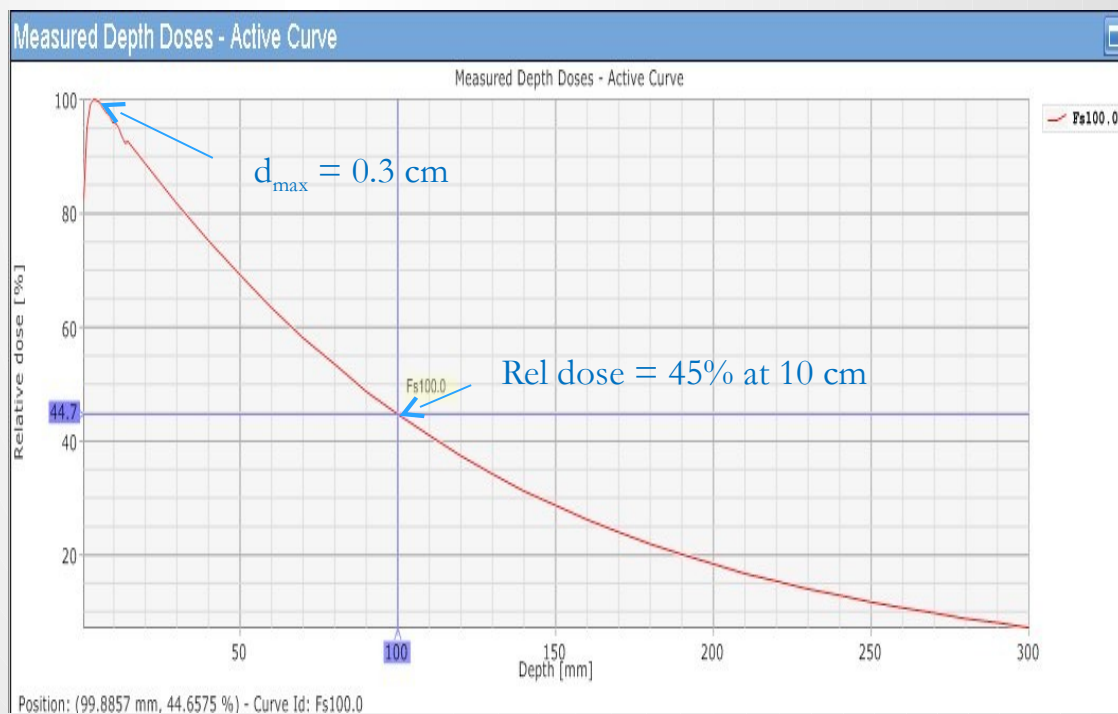


PDD

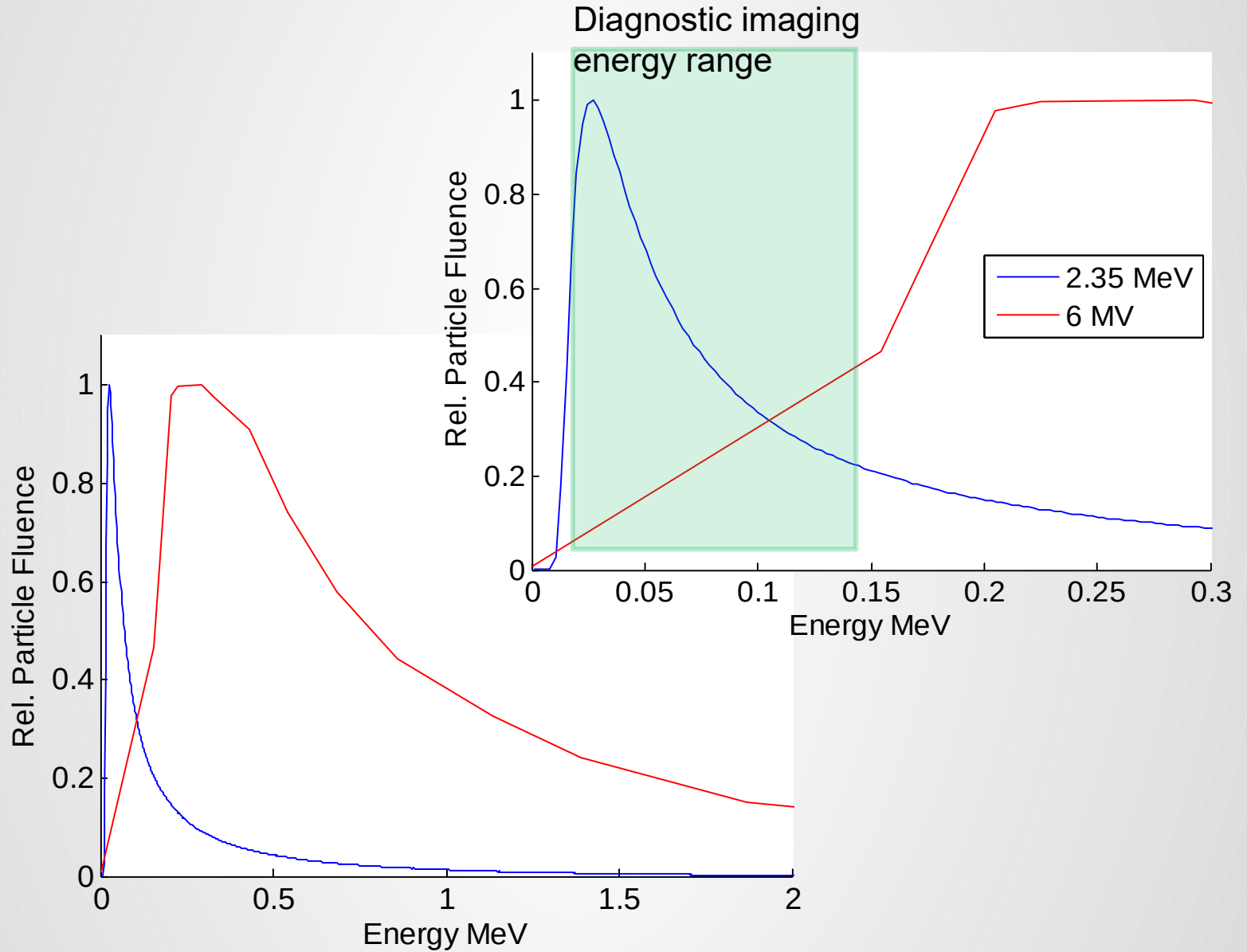
6 MV



2.35 MV

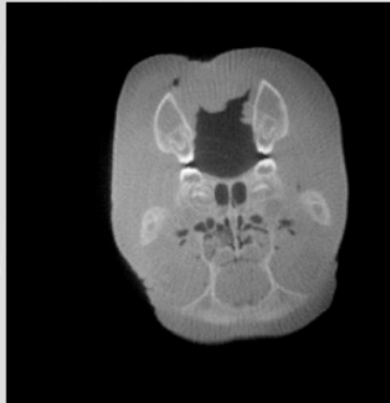


Compare energy spectra

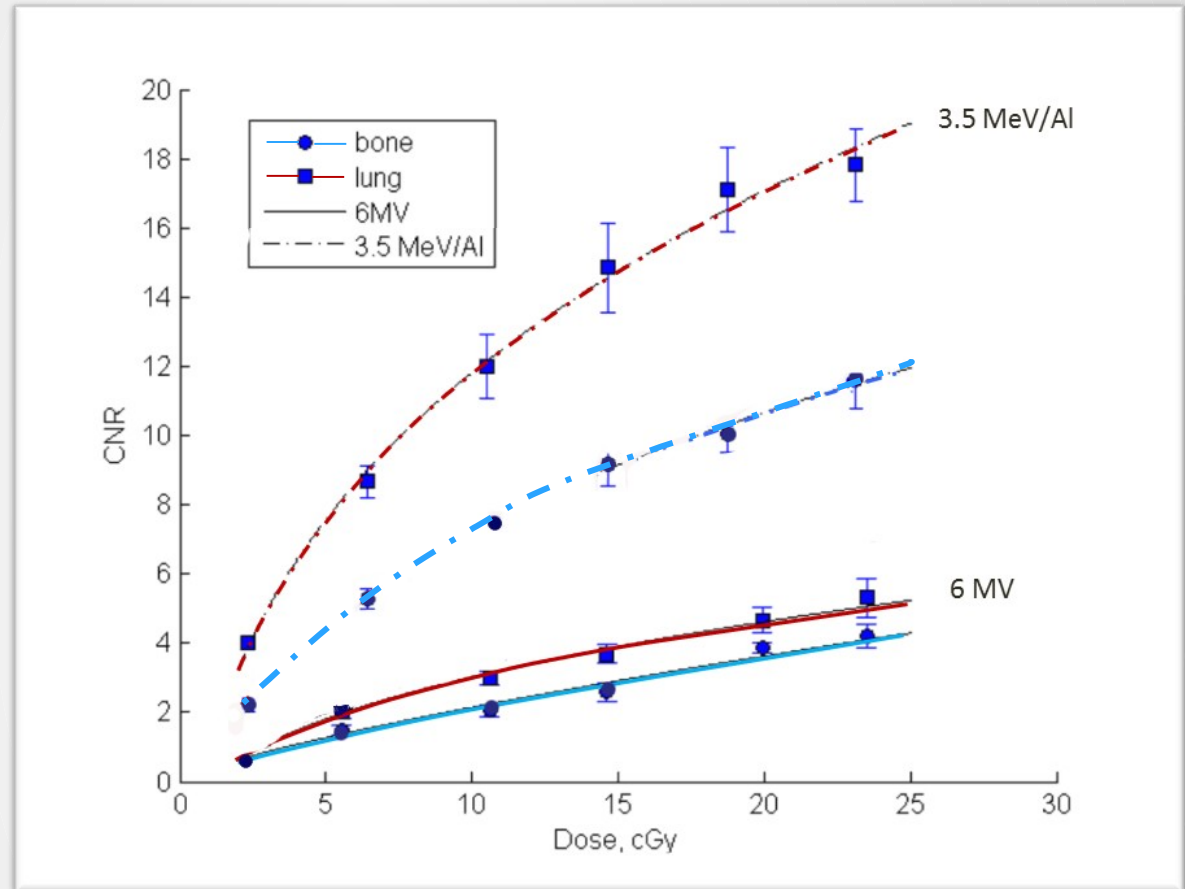
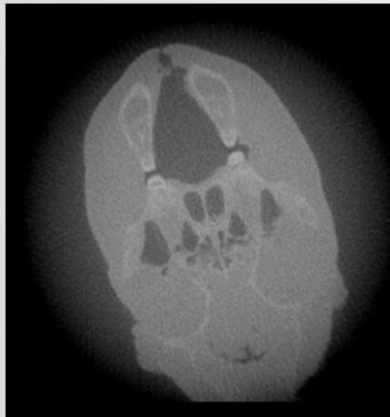


Low-Z CBCT: Contrast-to-noise

3.5 MeV/Al



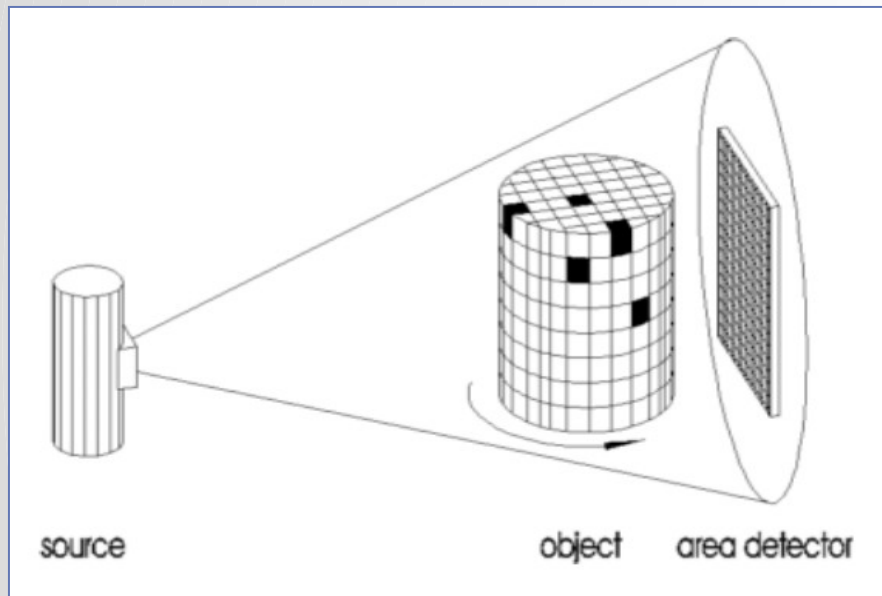
6 MV



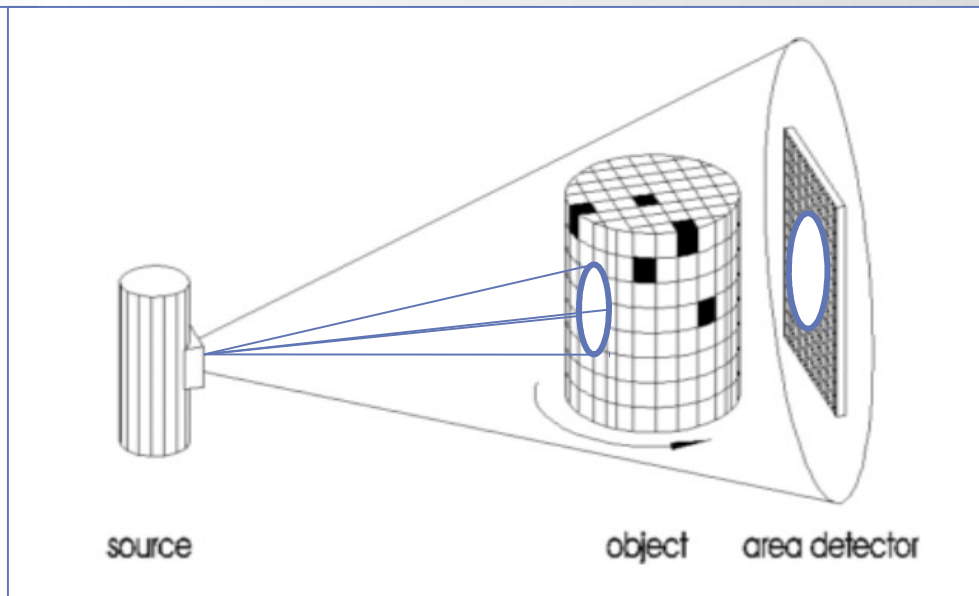
Decrease of dose with 3.5 MeV/Al beam compared to 6MV by a factor of ~5–8 depending on tissue and CNR

CBCT versus VOI CBCT

Full-Field (FF)



Volume-of-Interest (VOI)



Costs:

1. Imaging dose to entire volume of patient
2. Reduction of image quality due to scatter

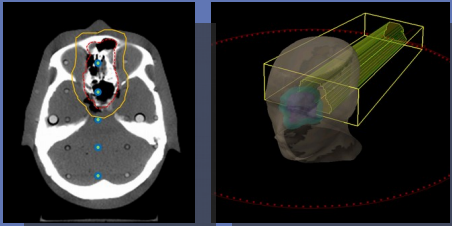
Benefits:

1. Localization of imaging dose to VOI
2. Improved scatter-to-primary characteristics

Low-Z VOI CBCT workflow

1

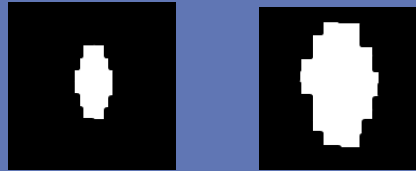
- Delineate VOI for imaging on planning CT
- Define CBCT arc geometry and beam shaping – export MLC sequence file



Eclipse 10.0

2

- Processing of MLC files using Matlab



Matlab

3

- Acquire 2.35 MV / Carbon target VOI CBCT



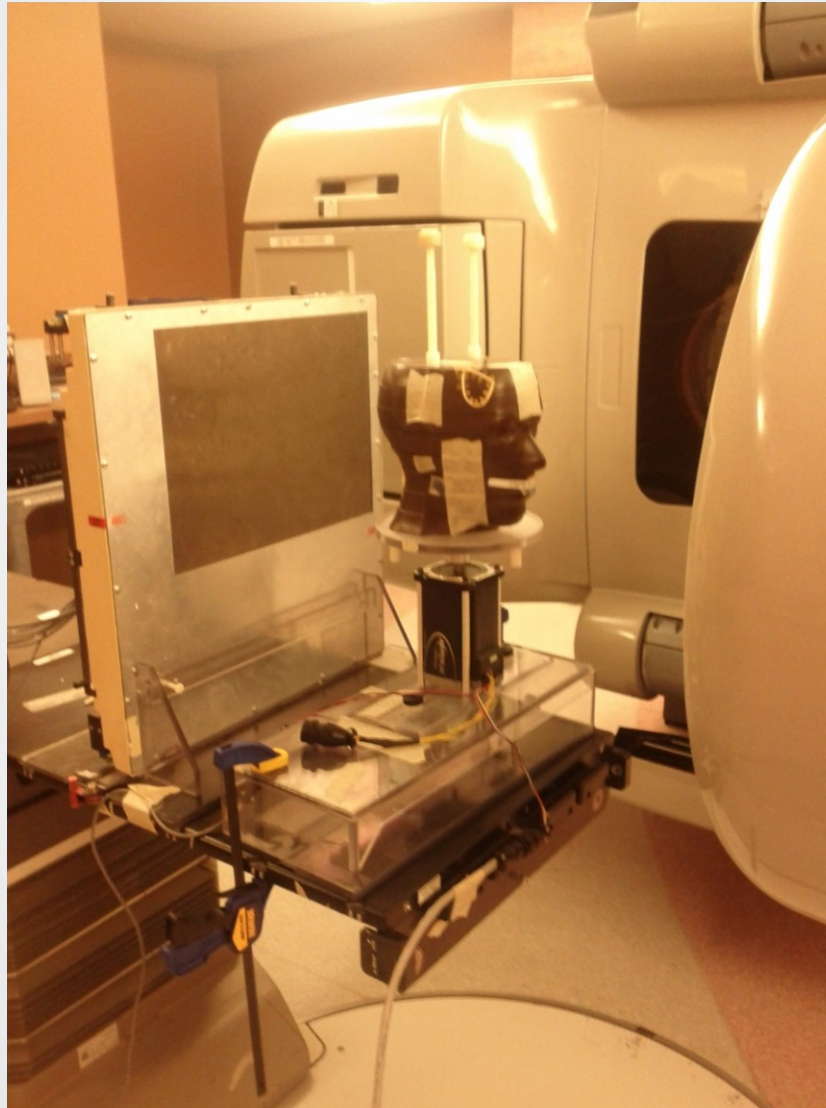
Clinac with carbon target

4

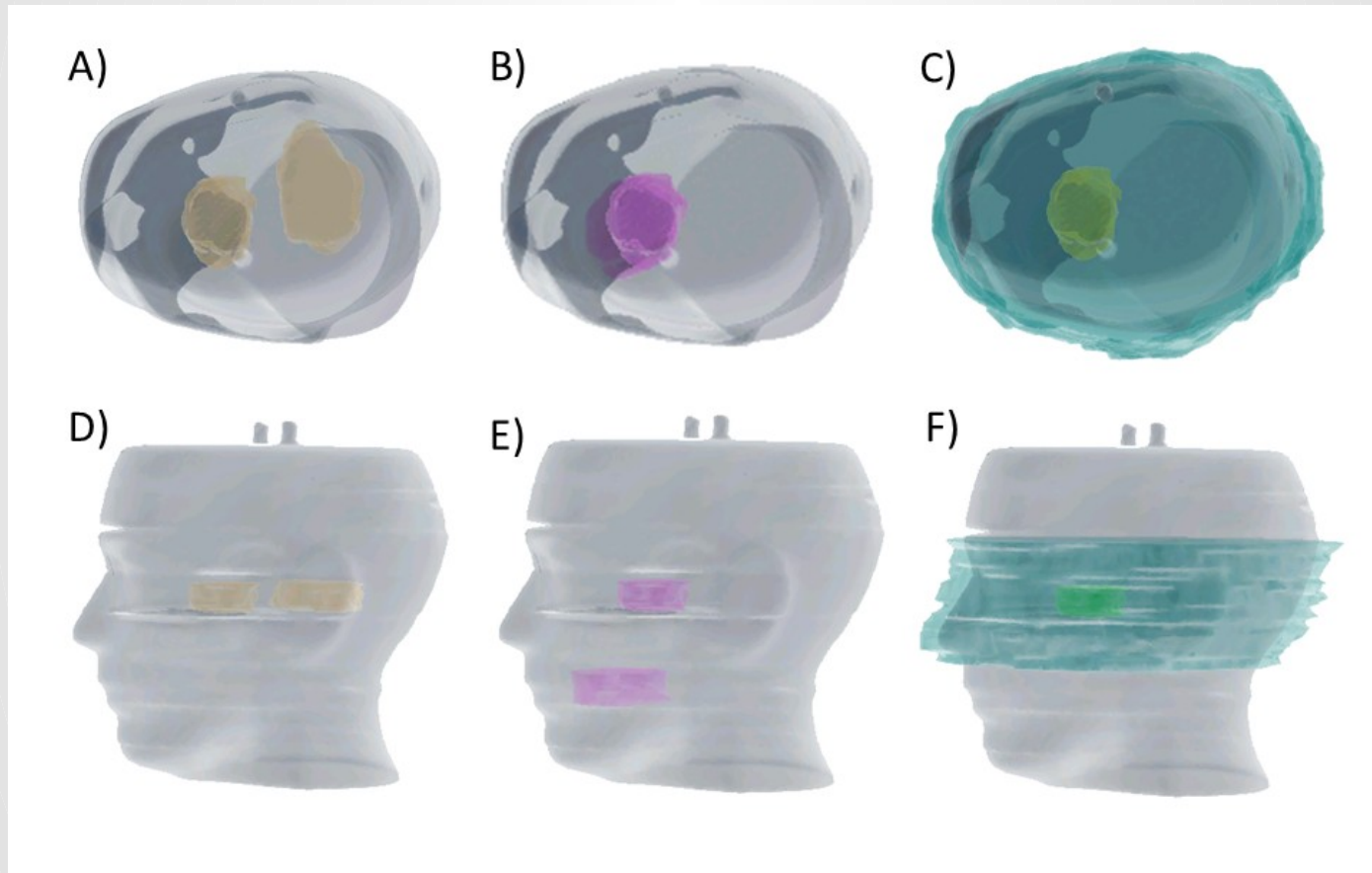
- FDK reconstruction
- Normalization

Reconstruction

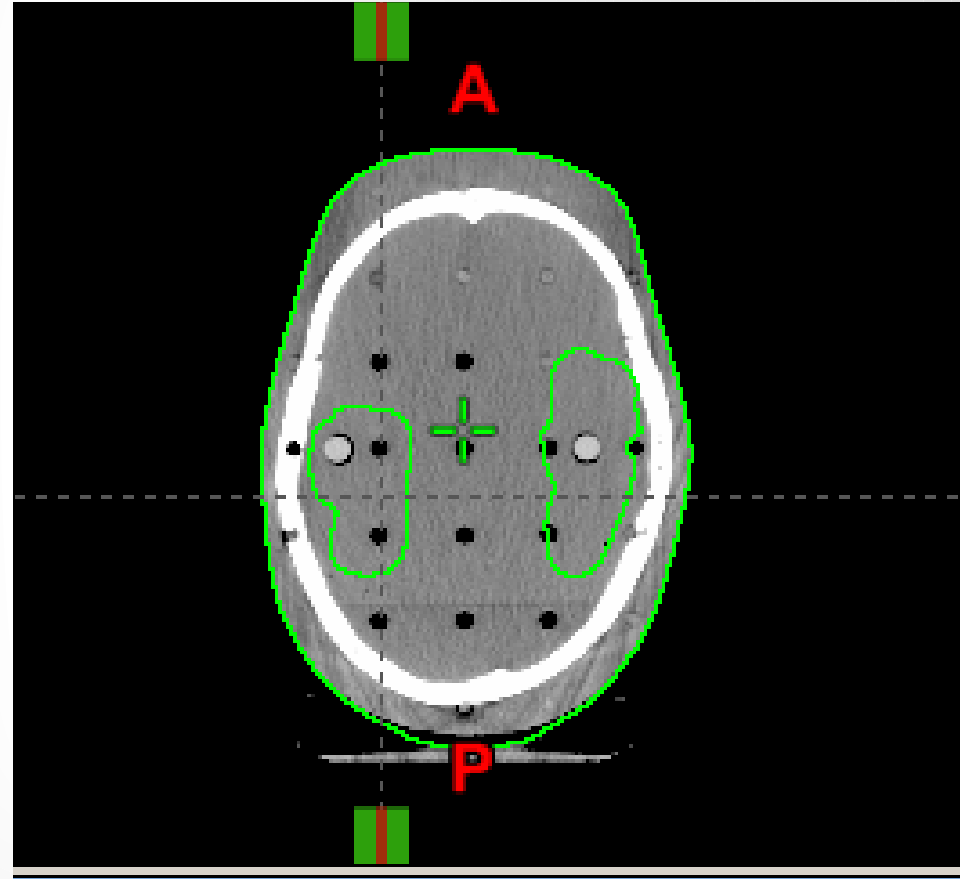
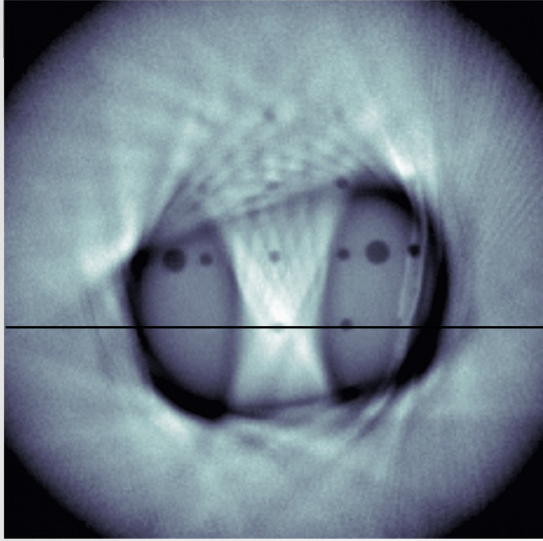
Apparatus



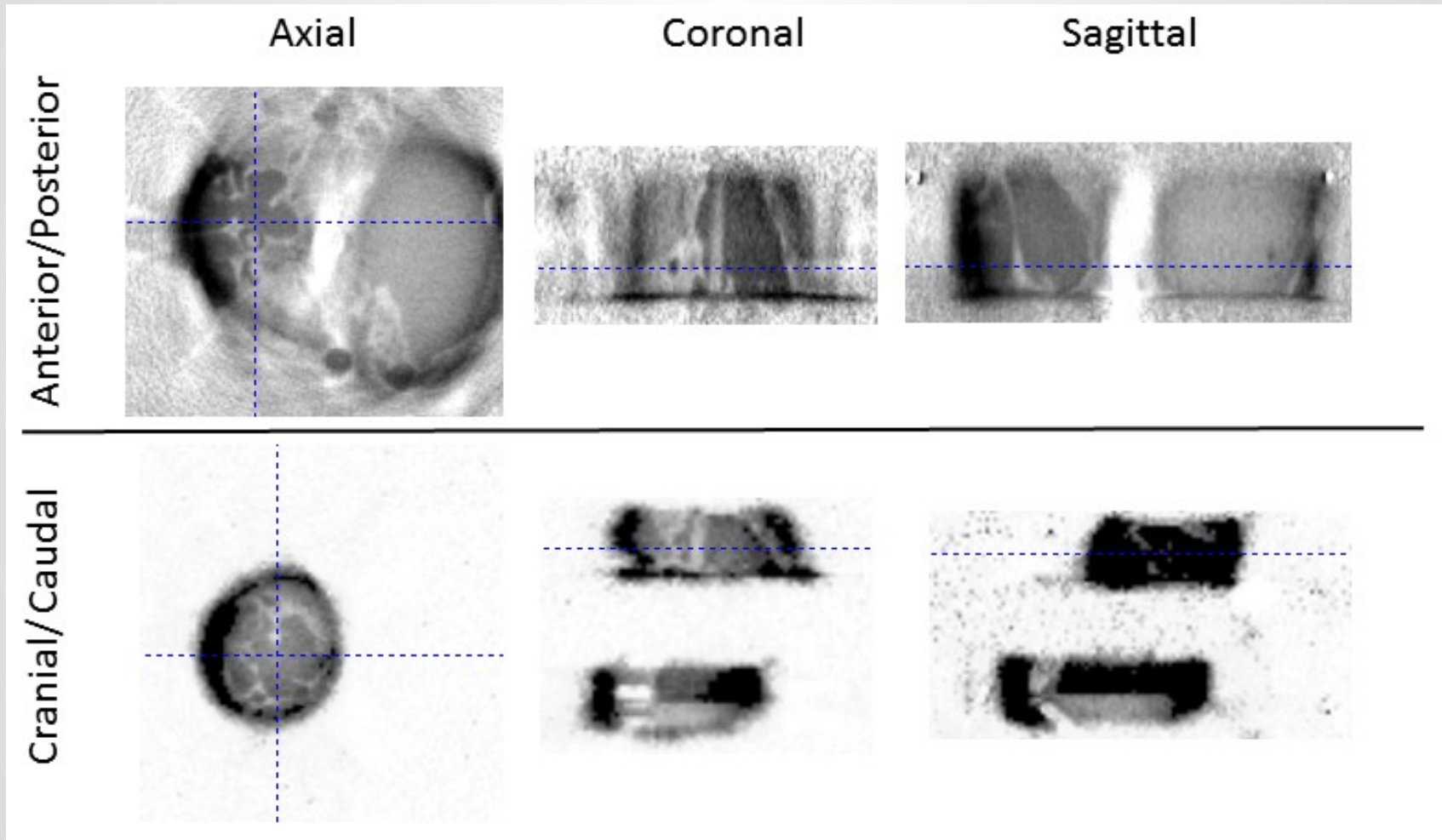
Example VOI configurations



Multiple VOIs



Multiple VOIs



Nested VOIs

Two separate MLC sequences merged together

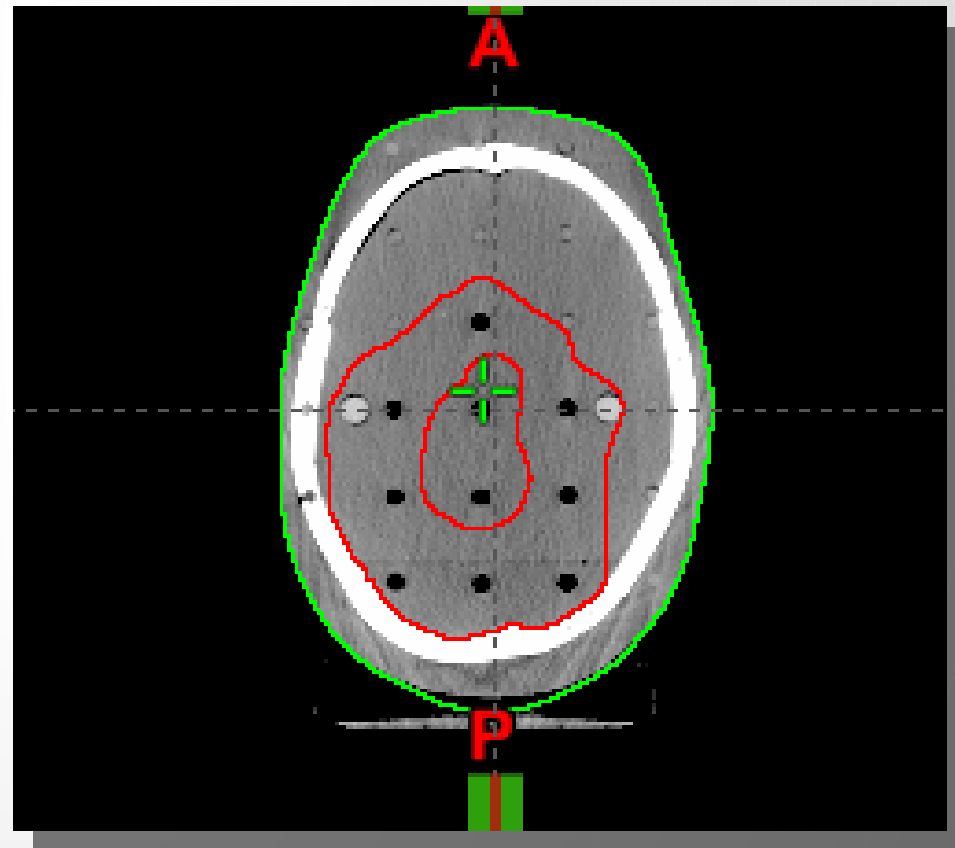
Define inner VOI

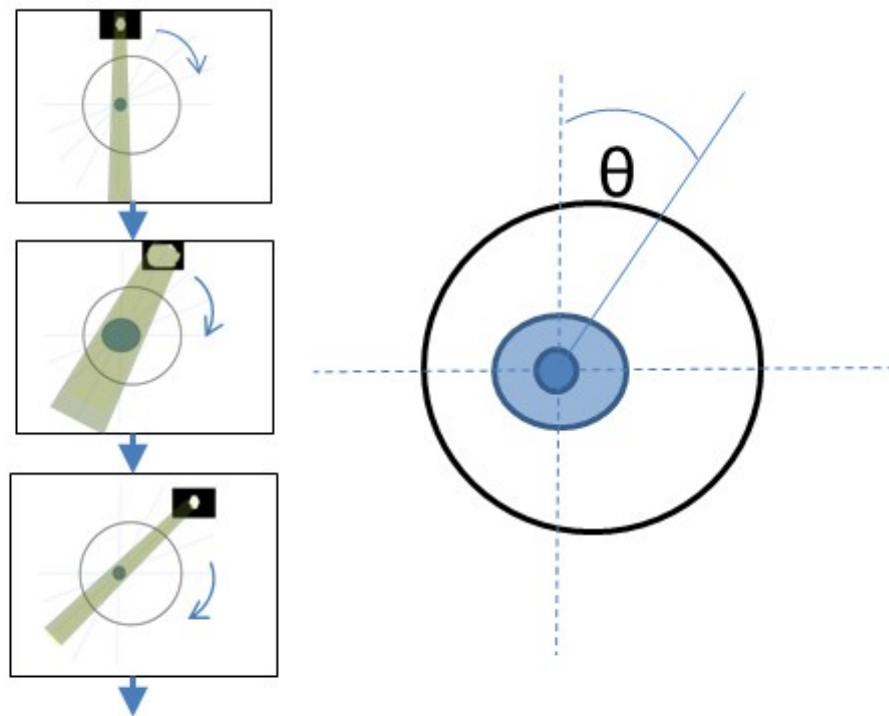
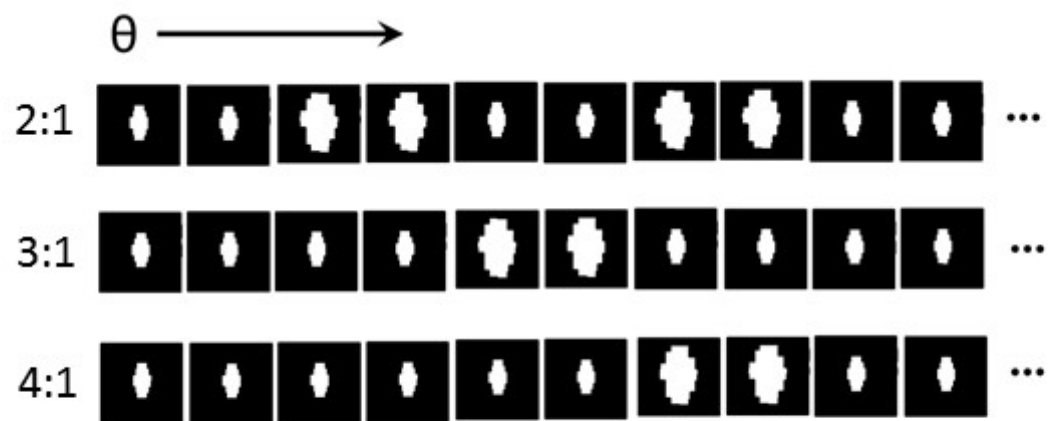
e.g. PTV

Define outer VOI

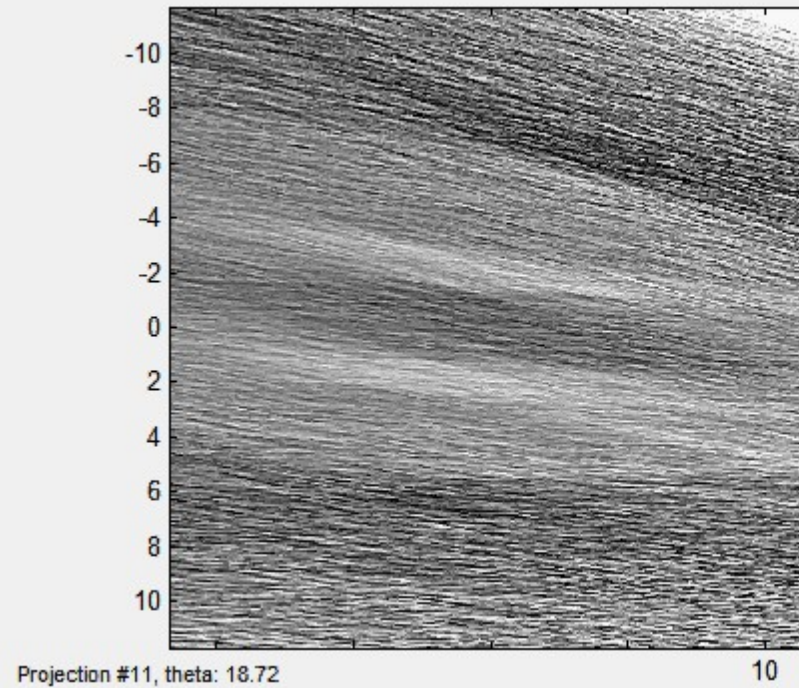
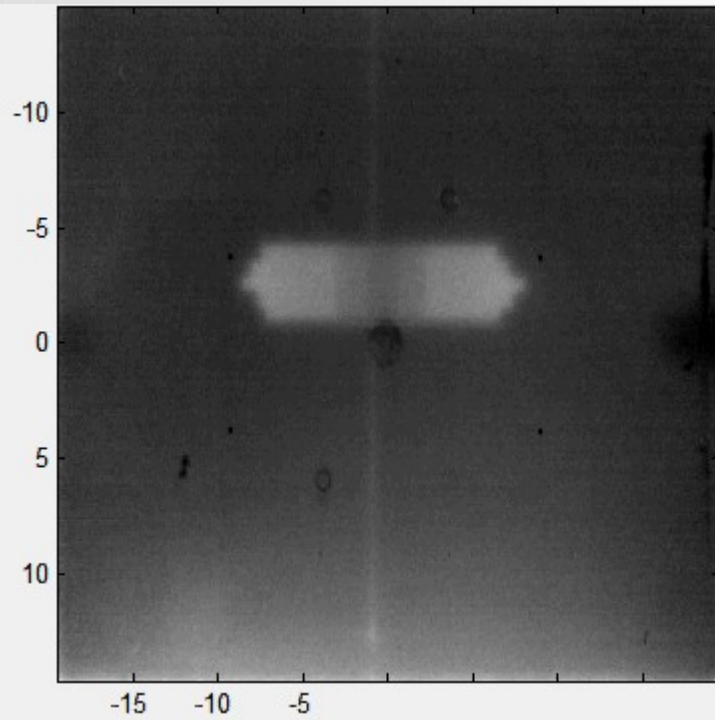
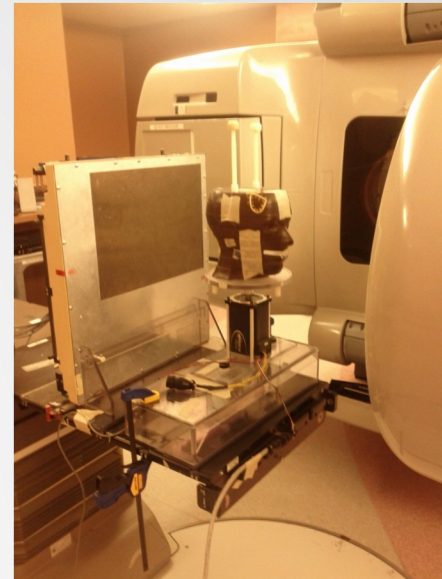
e.g. surrounding OARs or
body contour

Acquire inner VOI at higher
dose and CNR



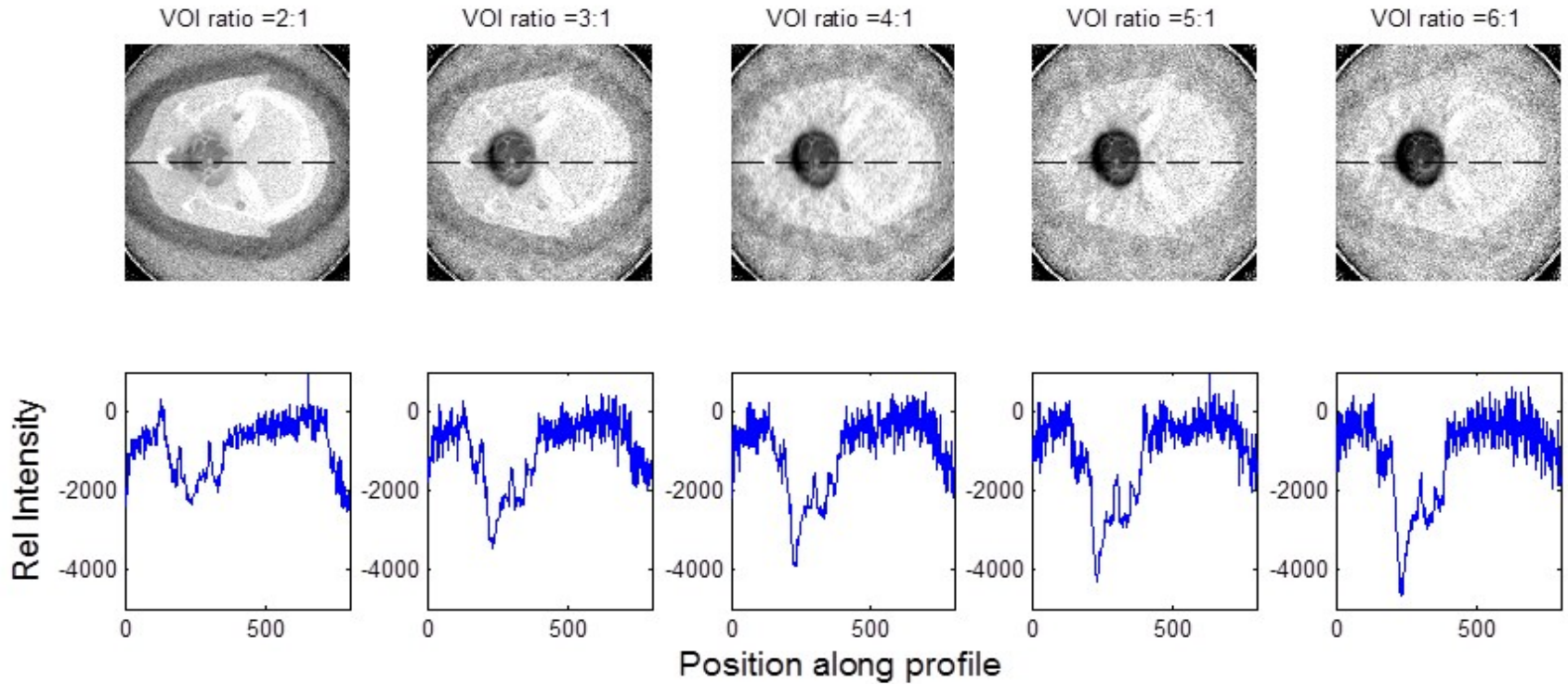
A**B**

Nested VOIs



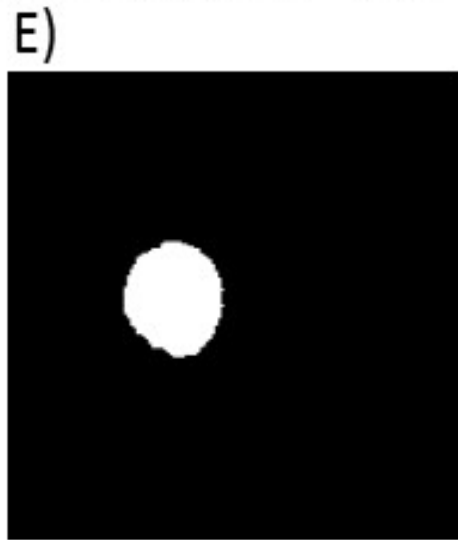
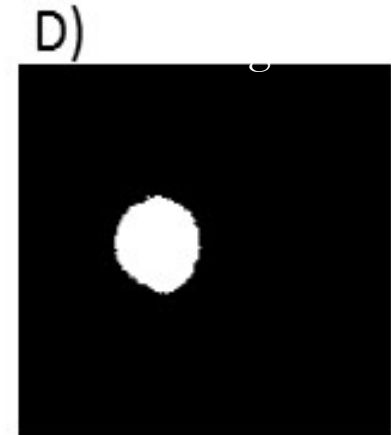
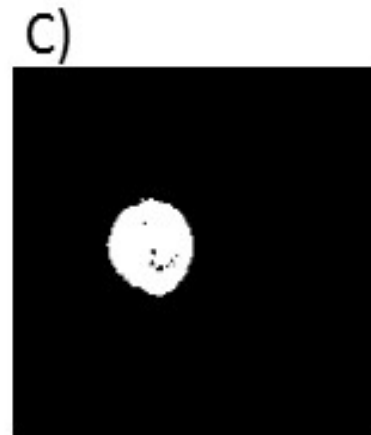
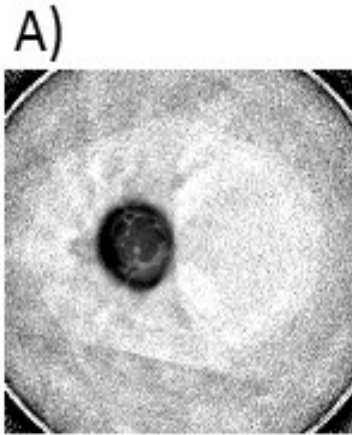
Projection #11, theta: 18.72

Raw reconstruction

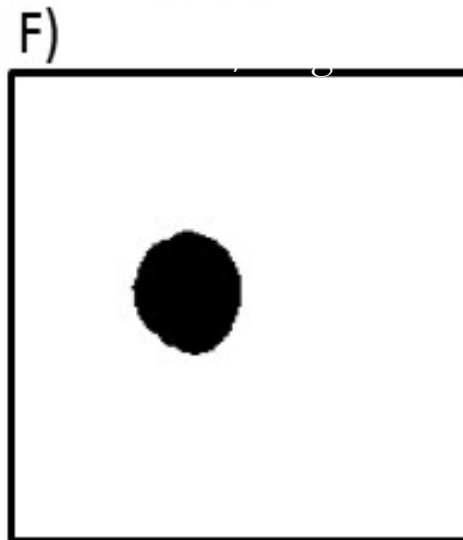


- Pixel intensities between the two VOIs now have different relative radiodensities
- For this reason we normalize inner and outer VOI after the reconstruction that can later be converted into Hounsfield units.

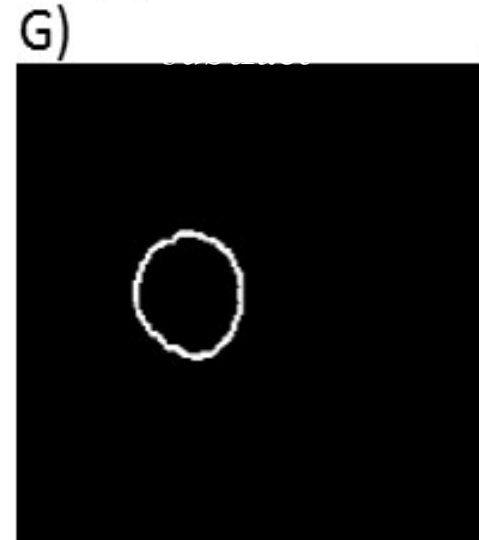
Normalize - masking



INNER MASK



OUTER MASK



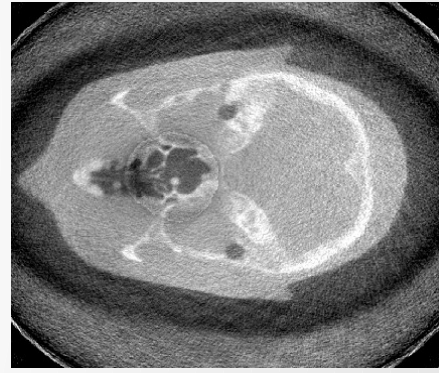
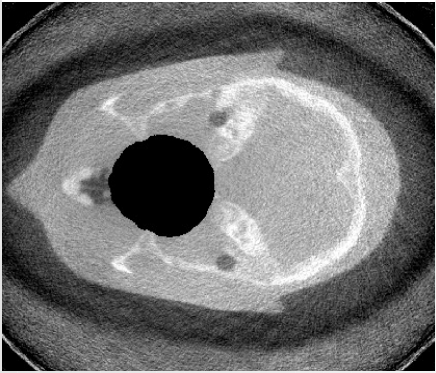
RING MASK

Normalize - masking

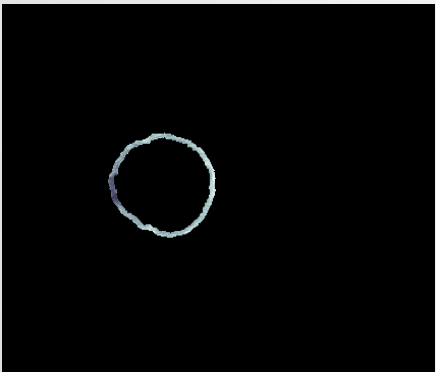
In



Out



Ring



Normalized reconstruction

2:1

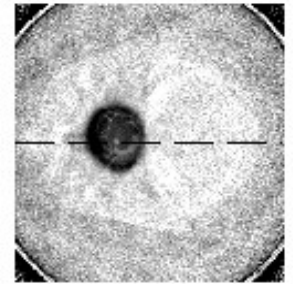
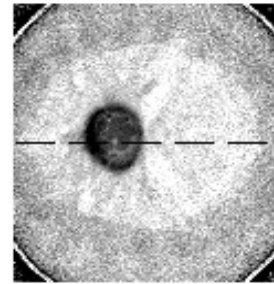
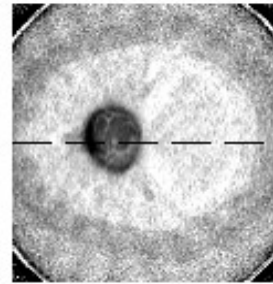
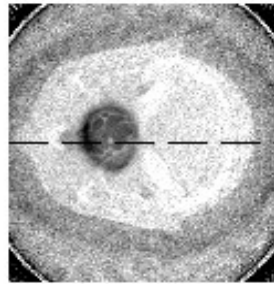
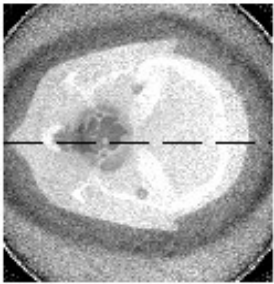
3:1

4:1

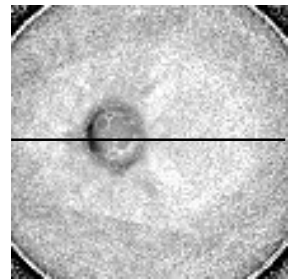
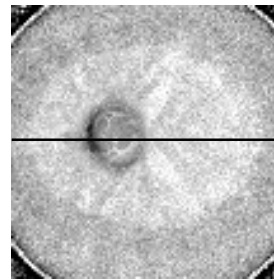
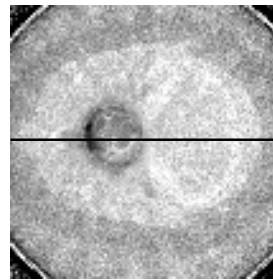
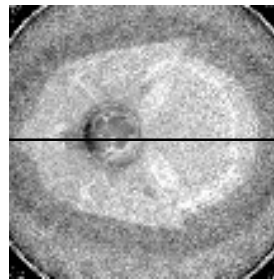
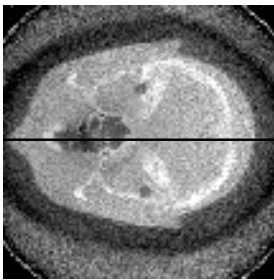
5:1

6:1

Raw

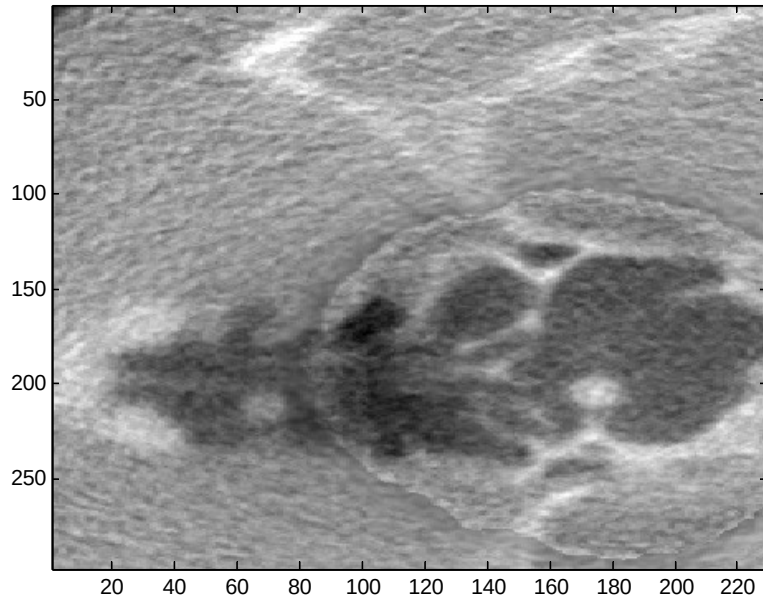


Normalized

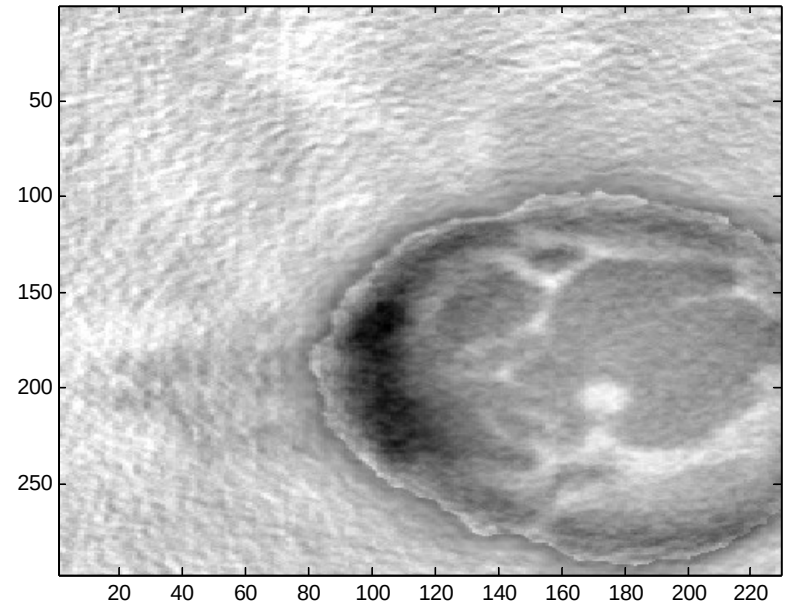


Zoomed images

2:1

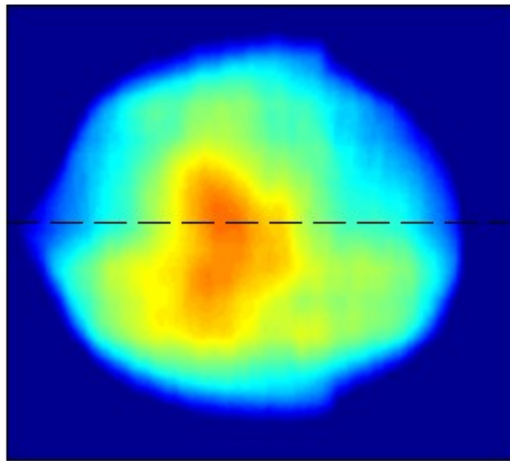


6:1

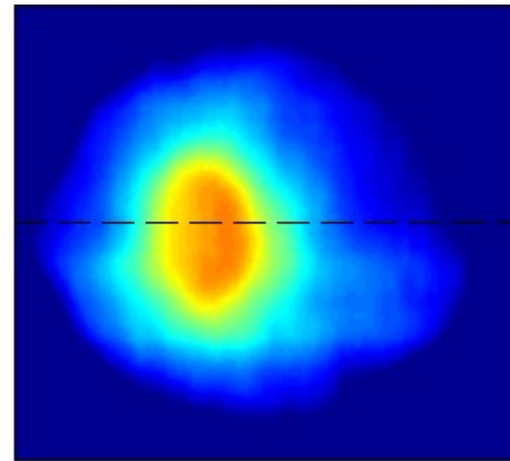


Radiochromic Film Dosimetry

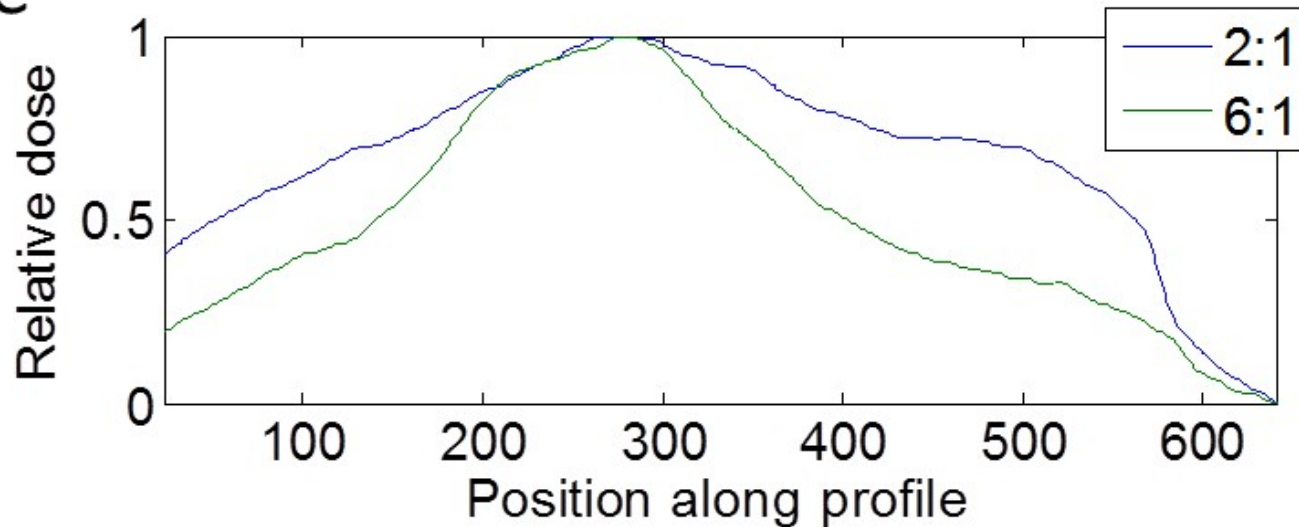
A



B

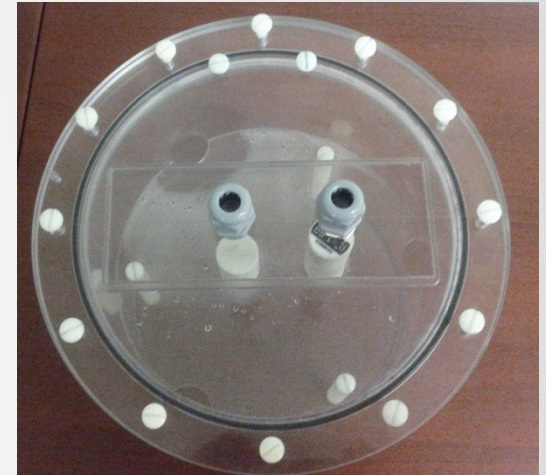
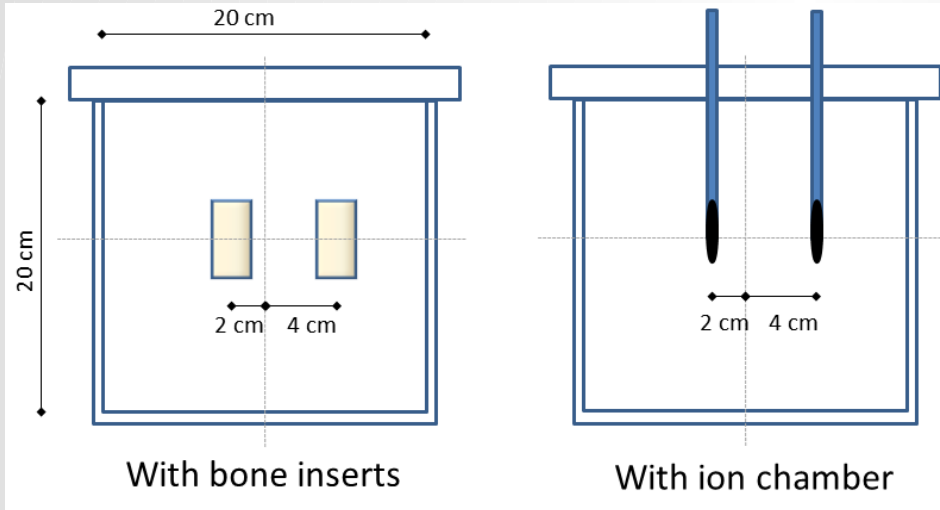


C



Find dose and CNR

Repeat the VOI sequences on a water phantom with cortical bone $\rho_e=1.69$ contrast tissue



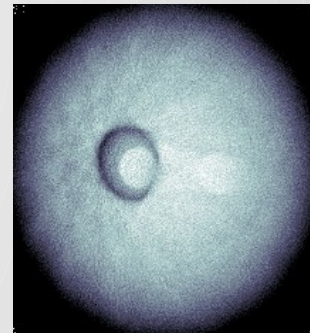
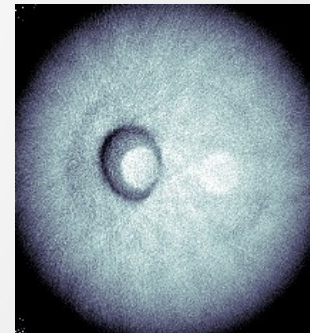
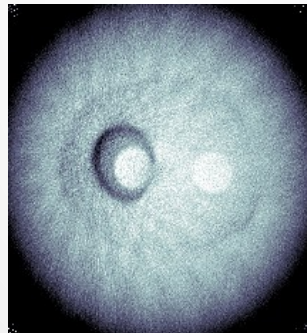
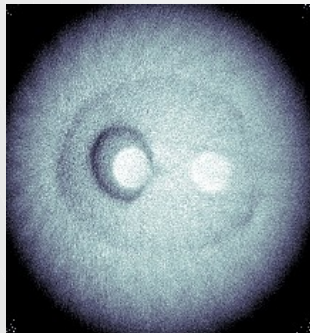
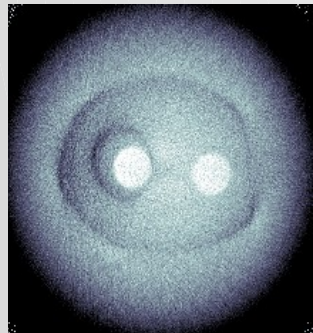
2:1

3:1

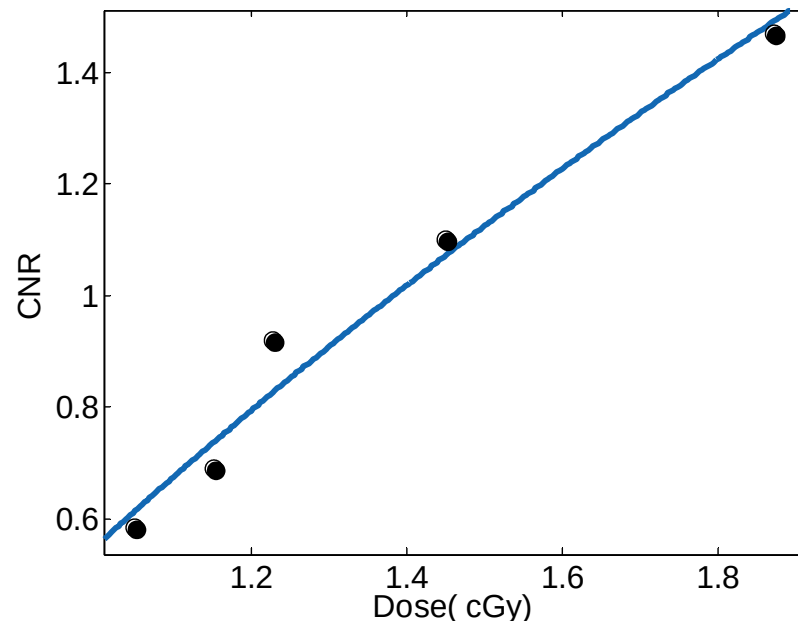
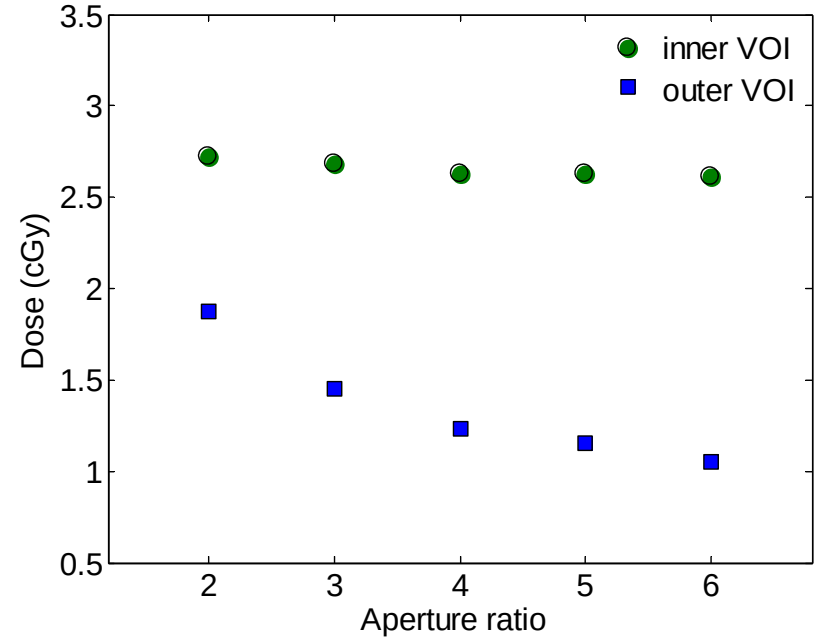
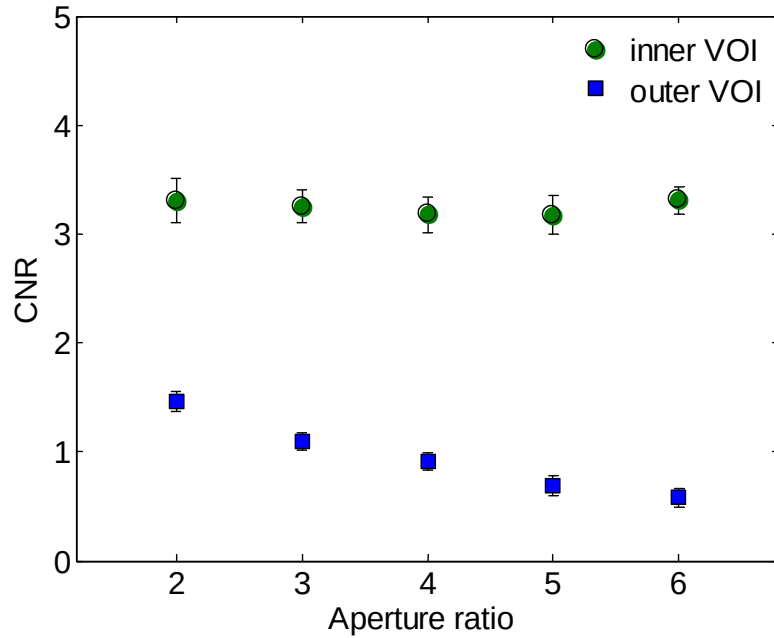
4:1

5:1

6:1



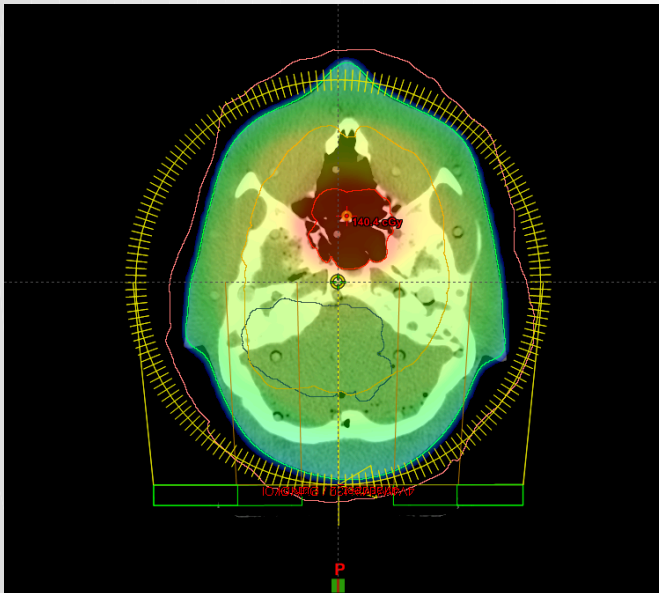
Control of dose and CNR in nested VOIs



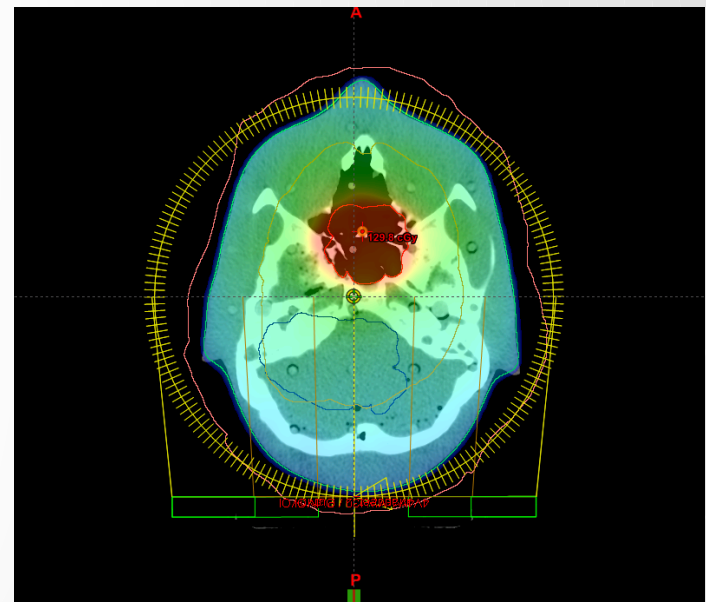
$$\text{CNR} = \frac{|P_{\text{bone}} - P_{\text{water}}|}{\sqrt{\sigma_{\text{bone}}^2 + \sigma_{\text{water}}^2}}$$

$$\text{CNR} \propto \sqrt{\text{dose}}$$

Low-Z CBCT dose AAA distributions

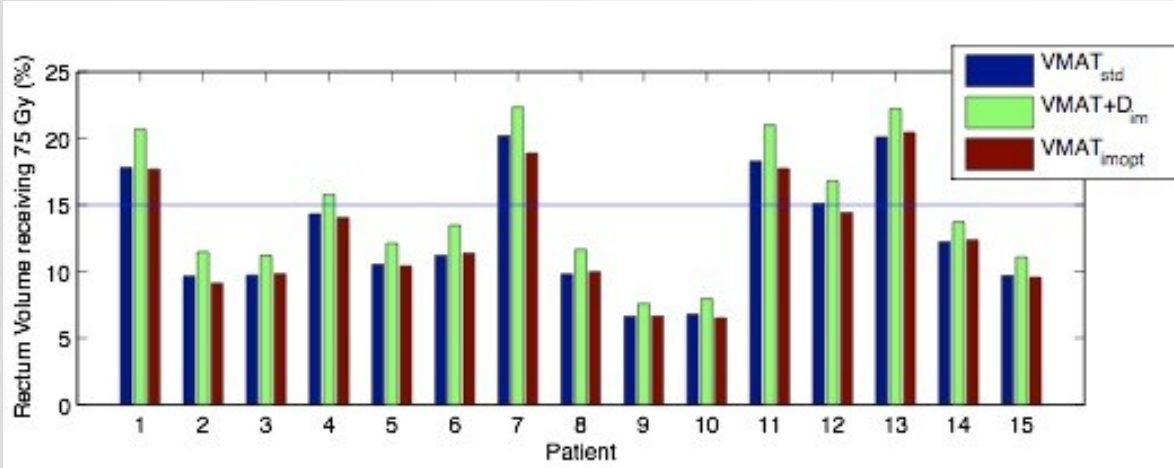


Nested VOI, 2:1

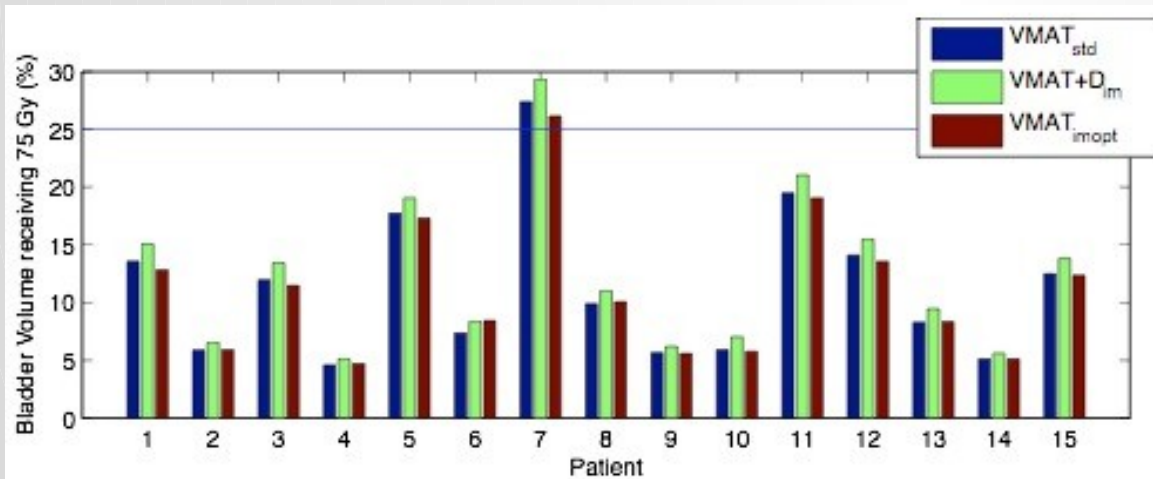


Nested VOI, 6:1

Case scenarios



Prostate cancer treatment
Based on QUANTEC review
For Rectum $V_{75} < 15\%$
For Bladder $V_{75} \leq 25\%$



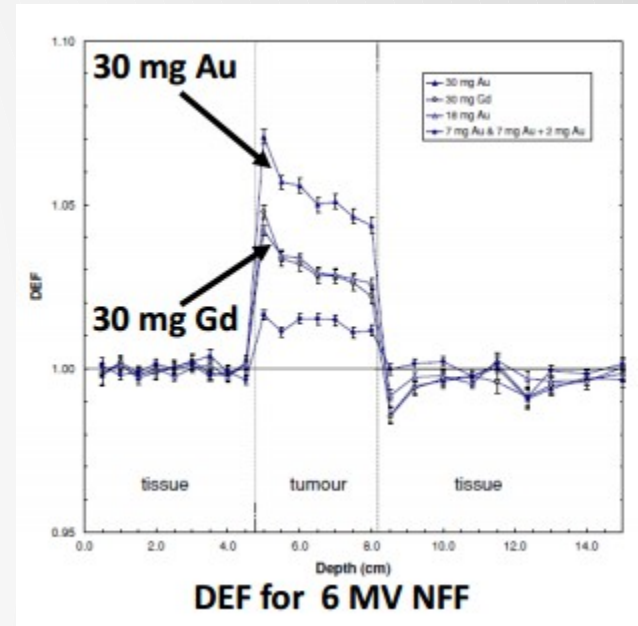
Summary

- Lowered dose and/or improved CNR by combining low-Z target beam with dose localization VOI approach
- Versatile MLC approach – multiple or nested VOIs possible as defined at planning step
- With VOI inner/outer ratio sequencing, dose reduction can be tuned to threshold CNR for outer VOI
- Dose can be calculated in Eclipse and subtracted from treatment dose

Future directions

Cho, S. (2005)

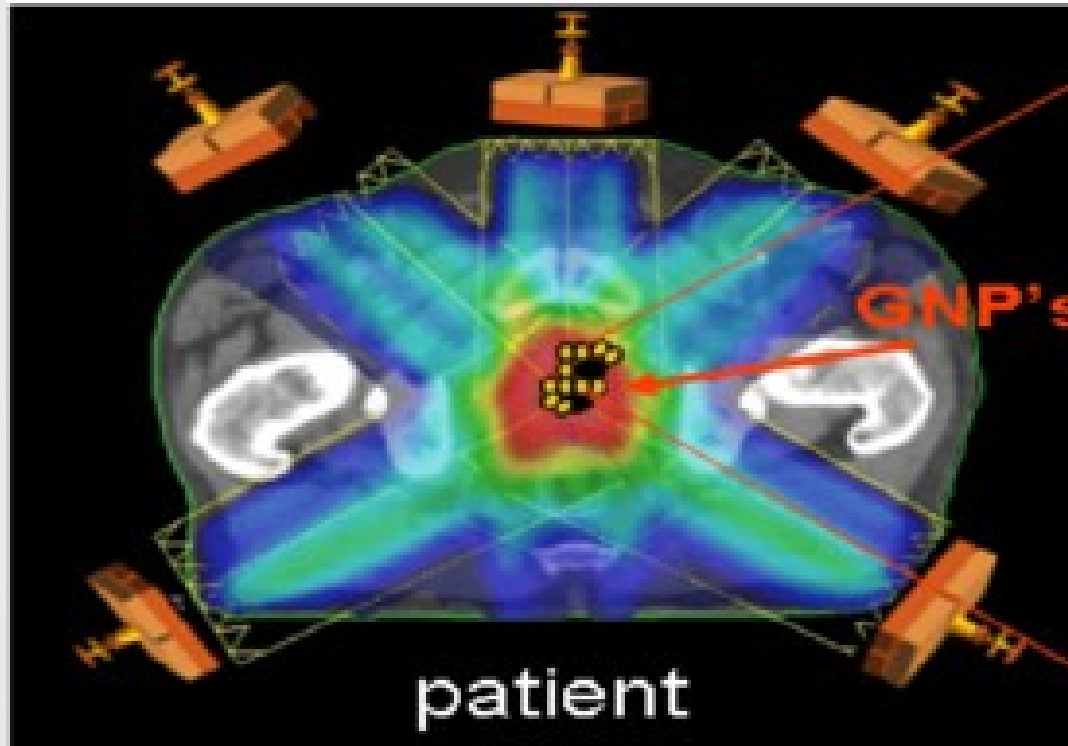
Based on the results of Hainfeld et al. (2004) simulated the dose enhancing using a modified phantom and tumor composition defined by ICRU to incorporate different concentrations of GNPs and compared 3 radiation sources.



Concentration (per gram of tumour)	140 kVp	6 MV FF	6 MV NFF	4 MV FF	4 MV NFF
7 mg Au	2.114	1.007	1.014	1.009	1.019
18 mg Au	3.811	1.015	1.032	1.019	1.044
30 mg Au	5.601	1.025	1.053	1.032	1.074

FF: flattening filter, NFF: no flattening filter.

Future directions



Thank you!

